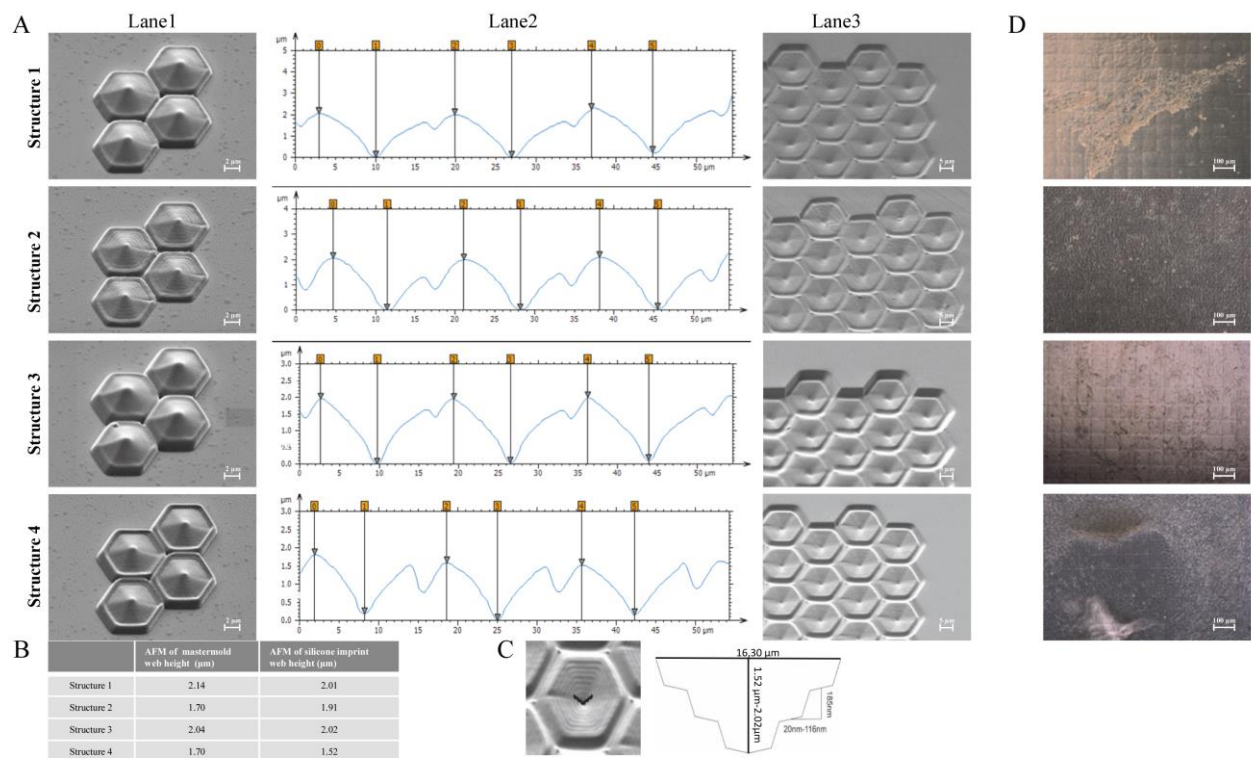


1 **SDC: Engineering of an artificial Descemet’s membrane**



2

3 SDC Figure 1: Engineering of an artificial Descemet’s membrane (DM) substrate by molding

4 the DM like topography (DLT) from an imprinted DM mastermold into silicone and

5 characterization of its surface topography and corneal endothelial cell (CEC) differentiation

6 impact.

7 A) SEM measurement of four, two-photon laser polymerized master structures with

8 defined inverted descemet like topography (DLT) differing in height and pitch angle in

9 μm and nm scale (lane 1). The four DLT structures were analyzed with confocal

10 microscopy (lane 2) and molded in silicone (lane 3).

11 B) Presentation of the molding accuracy of silicone from the master mold structures

12 measured by atomic force microscopy

13 C) 1000-fold magnification of the molded structure. The silicone imprints differed in
14 micro- and nanometer scale.

15 Adhesion of hMSC to each DLT structure induced changes of cell morphology from
16 fibroblastic-like into a polygonal shape compared to control cells on smooth silicone
17 between 2 and 5 days of cultivation. Further, in contrast to control cells cultured on the
18 smooth substrate, the cells cultivated on structures decreased all more or less in size in
19 dependency on the specific topography and changed their morphology. Interestingly,
20 each micro- and nanotopography induced a different cellular morphology and a different
21 macroscale behavior. Whereas the adhesion to structure 2 induced only marginal
22 changes in morphology, hMSC cultured on structures 3 and 4 changed morphology to a
23 polygonal shape and shrunk into 3D aggregates.

24 D) Only the adhesion on the silicone mold of Structure 1 enabled cells to build up 2D cell
25 associations instead of maintaining their fibroblastic morphology (Structure 2) or
26 staying in densely packaged 3D cell constructs (Structure 3 and 4).