

Appendix 1

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6th PeriOperative Quality Initiative in **DALLAS, TEXAS (2018)**

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Appendix 2: Search Terms

Searches done without an informatician

1. What physiologic information can NIRS provide? (This question combines queries about what NIRS actually measures as well as whether or not it can identify the lower limit of auto regulation [LLA] for brain perfusion?)

Search "near infrared spectroscopy" and "physiology" and "brain" (Filters: Review)

Results: 203

Screened: 203

Downloaded (4):

Search "near infrared spectroscopy" and "jugular venous" and "oxygen"

Results: 79

Screened: 79

Downloaded (10):

Search for "near infrared spectroscopy" and "LiCOX"

Results: 5

Screened: 5

Downloaded: 2

Search for "spectroscopy, near-infrared" AND "arterial pressure"

Results: 214

Screened: 214

Downloaded: 15 - Done

Search "spectroscopy, near-infrared" AND "brain" AND "blood flow velocity"

Results: 118

Screened: 118

Downloaded: 4

Search "spectroscopy, near-infrared" AND "brain" AND "methods" AND "standards"

Results: 44

Screened: 44

Downloaded: 0

Search "spectroscopy, near-infrared" AND "Neurophysiological Monitoring"

Results: 27

Screened: 27

Downloaded: 0

2. Do technical aspects of NIRS devices (the algorithm, optode spacing, wavelength selection) used to derive the StO₂ number matter?

Search "near infrared spectroscopy" and "optode spacing"

Results: 6

Screened: 6

Downloaded (0):

Search "oximetry" and "optode spacing"

Results: 3

Screened: 3

Downloaded (1):

Search "near infrared spectroscopy" and "wavelength selection"

Results: 73

Screened: 73

Downloaded (3):

3. During which components of the peri-operative period can NIRS be useful? (Pre-operative baseline helpful? Intraoperative, during cardiopulmonary bypass, post-operatively, both?)

Search "near infrared spectroscopy" and "preoperative" and "baseline"

Results: 36

Screened: 36

Download: 7

Search "near infrared spectroscopy" and "postoperative" and "baseline"

Results: 88

Screened: 88

Download: 2

Search "near infrared spectroscopy" and "postoperative" and "intensive care unit"

Results: 52

Screened: 52

Download: 6

4. Can using a NIRS-guided interventional algorithm reduce perioperative complications after [cardiac/high-risk non-cardiac] surgery?

Search "near infrared spectroscopy" and "surgery" and "stroke" and "acute kidney injury"

Results: 2

Screened: 2

Download: 0

Search "near infrared spectroscopy" and "surgery" and "stroke" (Filters: Clinical Trial)

Results: 11

Screened: 11

Download: 1

Search "cerebral oxygenation" and "surgery" and "stroke" (Filters: Clinical Trial)

Results: 9

Screened: 9

Download: 0

Search "cerebral oxygenation" and "surgery" and "acute kidney injury" (Filters: Clinical Trial)

Results: 1

Screened: 1

Download: 0

Search "near infrared spectroscopy" and "surgery" and "acute kidney injury" (Filters: Clinical Trial)

Results: 2

Screened: 2

Download: 0

Search "near infrared spectroscopy" and "randomized" and "surgery" (Filters: Clinical Trial)

Results: 94

Screened: 94

Download: 2

Searches done with an informatician

Search A (focused on Question 1)

Results 204

Screen 204

Downloaded 5

(near infrared spectroscop*[ti] OR near infrared spectromet*[ti] OR NIRS[ti] OR cNIRS[ti] OR NIR spectroscop*[ti] OR "Spectroscopy, Near-Infrared"[Majr])

AND (neuromonitor*[tiab] OR head[tiab] or crania*[tiab] or craniocerebral[tiab] or capitis[tiab] or craniu*[tiab] or cerebra*[tiab] or cerebru*[tiab] or brain*[tiab] or forebrain*[tiab] or skull*[tiab] or hemispher*[tiab] or intracran*[tiab] or encephal*[tiab])

AND

(physiolog*[ti] OR perfusion[ti] OR autoregulat*[ti] OR "cerebral blood flow"[ti] OR "mixed venous"[ti])

Search B (focused on Question 2)

Results 86

Screen 86

Downloaded 5

near infrared spectroscop*[ti] OR near infrared spectromet*[ti] OR NIRS[ti] OR cNIRS[ti] OR NIR spectroscop*[ti] OR "Spectroscopy, Near-Infrared"[Majr]) AND (neuromonitor*[tiab] OR head[tiab] or crania*[tiab] or craniocerebral[tiab] or capitis[tiab] or craniu*[tiab] or cerebra*[tiab] or cerebru*[tiab] or brain*[tiab] or forebrain*[tiab] or skull*[tiab] or hemispher*[tiab] or intracran*[tiab] or encephal*[tiab]) AND (optode*[tiab] OR wavelength[tiab] OR Invos*[tiab] OR "Covidien"[tiab] OR "Masimo"[tiab] OR "channels"[tiab])

Search C (focused on questions 3 and 4)

Results 56

Screen 56

Downloaded 11

(near infrared spectroscop*[ti] OR near infrared spectromet*[ti] OR NIRS[ti] OR cNIRS[ti] OR NIR spectroscop*[ti] OR "Spectroscopy, Near-Infrared"[Majr])

AND

(neuromonitor*[tiab] OR head[tiab] or crania*[tiab] or craniocerebral[tiab] or capitis[tiab] or craniu*[tiab] or cerebra*[tiab] or cerebru*[tiab] or brain*[tiab] or forebrain*[tiab] or skull*[tiab] or hemispher*[tiab] or intracran*[tiab] or encephal*[tiab])

AND

(randomized controlled trial[pt] OR controlled clinical trial[pt] OR randomized[tiab] OR placebo[tiab] OR clinical trials as topic[mesh:noexp] OR randomly[tiab] OR trial[ti])

Search D (focused on questions 3 and 4)

Results 25

Screen 25

Downloaded 9

(near infrared spectroscop*[ti] OR near infrared spectromet*[ti] OR NIRS[ti] OR cNIRS[ti] OR NIR spectroscop*[ti] OR "Spectroscopy, Near-Infrared"[Majr])

AND

(operati*[tiab] or perioperat*[tiab] or peroperat*[tiab] or preoperati*[tiab] or postoperat*[tiab] or intraoperat*[tiab] or surg*[tiab] OR "Perioperative Period"[Mesh] OR "Perioperative Care"[Mesh])

AND

("Cardiac Surgical Procedures"[Majr] OR cardiac*[tiab] OR heart[tiab] OR "Cardiopulmonary Bypass"[Mesh] OR "cardiopulmonary bypass"[tiab])

AND

(randomized controlled trial[pt] OR controlled clinical trial[pt] OR randomized[tiab] OR placebo[tiab] OR clinical trials as topic[mesh:noexp] OR randomly[tiab] OR trial[ti])

Search E (focused on questions 3 and 4)

Results 107

Screen 107

Downloaded 14

(near infrared spectroscop*[tiab] OR near infrared spectromet*[tiab] OR NIRS[tiab] OR cNIRS[tiab] OR NIR spectroscop*[tiab] OR "Spectroscopy, Near-Infrared"[Majr])

AND

(neuromonitor*[tiab] OR head[tiab] or crania*[tiab] or craniocerebral[tiab] or capitis[tiab] or craniu*[tiab] or cerebra*[tiab] or cerebru*[tiab] or brain*[tiab] or forebrain*[tiab] or skull*[tiab] or hemispher*[tiab] or intracran*[tiab] or encephal*[tiab])

AND

(operati*[tiab] or perioperat*[tiab] or peroperat*[tiab] or preoperati*[tiab] or postoperat*[tiab] or intraoperat*[tiab] or surg*[tiab] OR "Perioperative Period"[Mesh] OR "Perioperative Care"[Mesh])

AND

(randomized controlled trial[pt] OR controlled clinical trial[pt] OR randomized[tiab] OR placebo[tiab] OR clinical trials as topic[mesh:noexp] OR randomly[tiab] OR trial[ti])

Appendix 3: Detailed Description of Near-Infrared Spectroscopy (NIRS) Devices

The complexity of cerebral blood flow as well as the devices designed to measure ScO₂ require a working knowledge of both brain physiology and the scientific principles of NIRS in order to use cerebral oximetry effectively. Blood flow to the brain is a function of driving pressure and resistance, in accordance with the **Hagen-Poiseuille law**.^{1,2} Because of its importance, the human brain has developed the ability to autoregulate blood flow within the “cerebral autoregulatory range” – within this range of perfusion pressures, the brain can modify regional vascular resistance (RVR) in order to keep blood flow relatively constant.³ As with all tissues, the brain contains arteries, capillaries, and veins and the blood that is present in the brain can be divided into these three theoretical compartments.⁴ Changes in cerebral vascular tone that impact RVR also change vessel compliance, which can alter the ratio of these compartments.⁵ Variables that affect cerebral RVR include PaCO₂, pH, and extreme hypoxia **[Figure 1]**.⁶ Changes in adrenergic tone as well as temperature can also impact cerebral RVR although the mechanism(s) are incompletely understood and in some cases, controversial.⁶⁻⁸

The ultimate physiologic goal of a cerebral oximeter is to give the user some indirect indication of the cerebral tissue oxygen saturation (SctO₂). This makes cerebral oximetry different from pulse oximetry, the goal of which is to determine the oxygen saturation in arterial *blood*. Because blood (i.e., hemoglobin) oxygenation is not a direct measure of tissue oxygenation, early cerebral oximeters attempted to measure the oxidation state of cytochrome aa₃, the terminal component of the mitochondrial electron chain (called Cyt_{ox}).⁹ In theory, Cyt_{ox} could provide investigators (and clinicians) with information regarding the adequacy of oxygen supply and demand in brain tissue itself.

Unfortunately, because of cytochrome aa₃ exists in lower concentrations than hemoglobin and because it more weakly absorbs near infrared (NIR) radiation, accurately measuring Cyto_x is challenging and requires broadband devices which are not available for clinical use.¹⁰

Cerebral oximetry utilizes NIRS to measure the relative concentration of “chromophores” (i.e., biological molecules that absorb electromagnetic radiation [EMR]), based on the modified Beer-Lambert Law for a scattering medium which states^{11,12}:

$$OD_{\lambda} = \varepsilon_{\lambda} \bullet L \bullet c \bullet DPF + OD_{R,\lambda},$$

where, OD_{λ} is the optical density of a medium, ε_{λ} represents the extinction coefficient of a chromophore, L represents the source-detector separation, c represents the concentration of the chromophore, DPF (differential pathlength factor) represents a correction factor designed to estimate how far a photon actually travels through tissue, and $OD_{R,\lambda}$ represents a geometry and wavelength-dependent correction factor. Of note DPF is dependent on the absorption coefficient of tissue, the scattering coefficient, and L , and is wavelength-dependent.¹³ When *changes* in concentration are desired, this equation can be simplified to $\Delta c = \Delta OD_{\lambda} / (\varepsilon_{\lambda} \bullet L \bullet DPF)$ for one chromophore as OD_R is a constant and drops out. To determine the concentration of multiple chromophores (e.g., oxyhemoglobin and deoxyhemoglobin), a set of equations (one for each wavelength) can be solved simultaneously using matrix algebra [**Figure 2**]. Of note, actual concentrations of chromophores cannot be measured unless ε_{λ} , L , and DPF are known. While some research devices are capable of estimating the DPF and providing absolute measures of chromophore concentrations, FDA-approved devices are not.¹⁴ *Therefore, cerebral oximetry measurements must be viewed as relative measures, not*

absolute values. Accordingly, the changes in SctO₂ relative to baseline (i.e., pre-induction of anesthesia) measurements offer more clinical information that complements absolute measurements.

Modern cerebral oximeters use spatially resolved spectroscopy (SRS) to focus their measurements on the brain. EMR is transmitted into the brain through the skull, and photons travel in stochastic (predictable only on a probabilistic basis) fashion through skin, muscle, fat, bone (skull), meninges, and brain. Photon detectors (e.g. photodiodes) are placed 2-4 cm away from the light source, serving to detect photons that are reflected by tissues in their path. In order to separate the absorbance of the brain chromophores from the absorbance of other extracranial tissue chromophores, the stronger, more proximal signal (lower absorbance) is subtracted from the weaker distal signal (higher absorbance). Both signals are affected equally by skin, muscle, fat, and bone, and the difference between the two signals is therefore due to absorbance through the brain.¹⁵ **[Figure 3]**

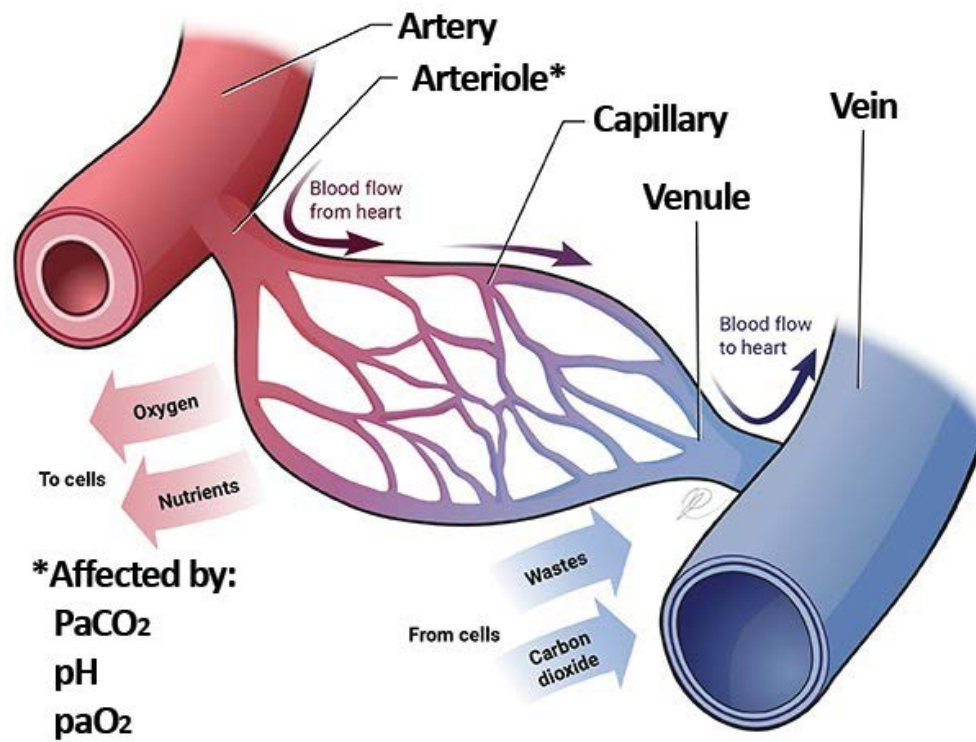
As noted in the manuscript, commercially available cerebral oximeters are therefore only capable of measuring the relative amount of oxygenated hemoglobin in an “optical field” interrogated using SRS-NIRS. Furthermore, SRS-NIRS analyzes all light absorbed by the brain and other tissues, as compared to pulse oximeters which only analyze pulsatile (arterial) absorbance. The “tissue saturation” of the blood in the brain measured by a cerebral oximeter is a combination of arterial, capillary, and venous blood. If one assumes that arterial oxygen saturation is close to 100%, that the volume of capillary blood is relatively small, and that the relative volume (or ratio) of arterial and venous blood is fixed (e.g. 30:70, or 25:75, depending on the device

manufacturer), the oxygenation of venous blood leaving the cerebral capillary beds can be estimated using the following equation:

$$S_{\text{venous,cerebral}}O_2 = (S_{\text{tissue}}O_2 - 0.3*100\%)/(0.7)$$

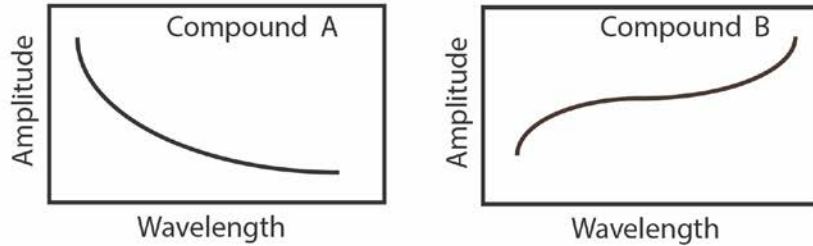
In fact, commercially available cerebral oximeters are often validated against measurements of jugular bulb oxygen saturation during staged hypoxia protocols or in patients requiring extracorporeal support.^{16,17} In that sense, they could be more accurately viewed as non-invasive jugular venous bulb monitors, not tissue oximeters per se. Indeed, direct comparisons of cerebral or jugular hemoglobin saturation and brain tissue PO₂ using invasive measures (Clarke electrode) have found very little relationship between the two.¹⁸⁻²⁰ Therefore, as stated above, commercially available cerebral oximeters all assume a fixed arterial:venous ratio (the true percentage of venous blood can range from 33-84%) and the arterial:venous ratio is affected by many variables.^{5,21,22}

Appendix 3, Figure 1



Appendix 3 , Figure 2

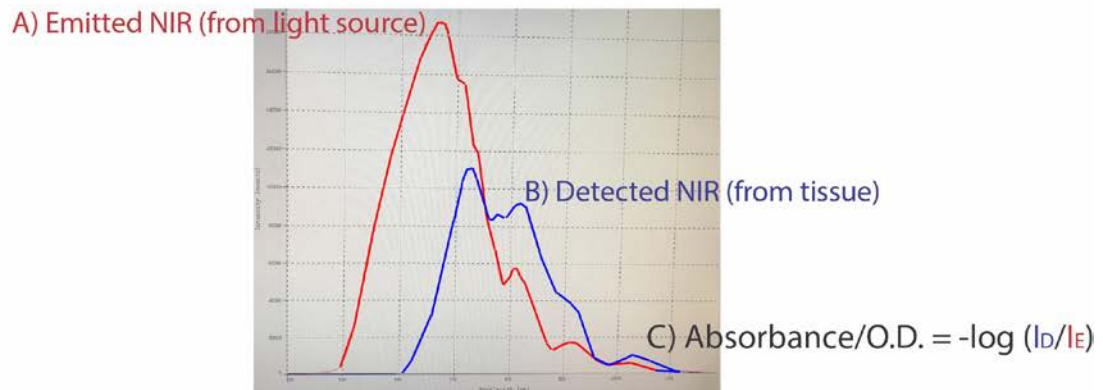
1) Each Chromophore Produces A Unique Spectrum



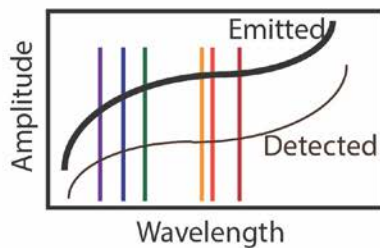
2) These Can Be Mathematically Combined Using Matrix Algebra

$$\begin{pmatrix} \text{Compound A} \\ \text{Compound B} \end{pmatrix} = \begin{pmatrix} c_{11} & c_{12} & c_{13} & c_{14} & c_{15} & c_{16} \\ c_{21} & c_{22} & c_{23} & c_{24} & c_{25} & c_{26} \end{pmatrix} \times \begin{pmatrix} \text{OD1} \\ \text{OD2} \\ \text{OD3} \\ \text{OD4} \\ \text{OD5} \\ \text{OD6} \end{pmatrix}$$

3) By Transmitting and Recording Light Into Tissue, Absorbance / Optical Density Can Be Measured at Each Wavelength



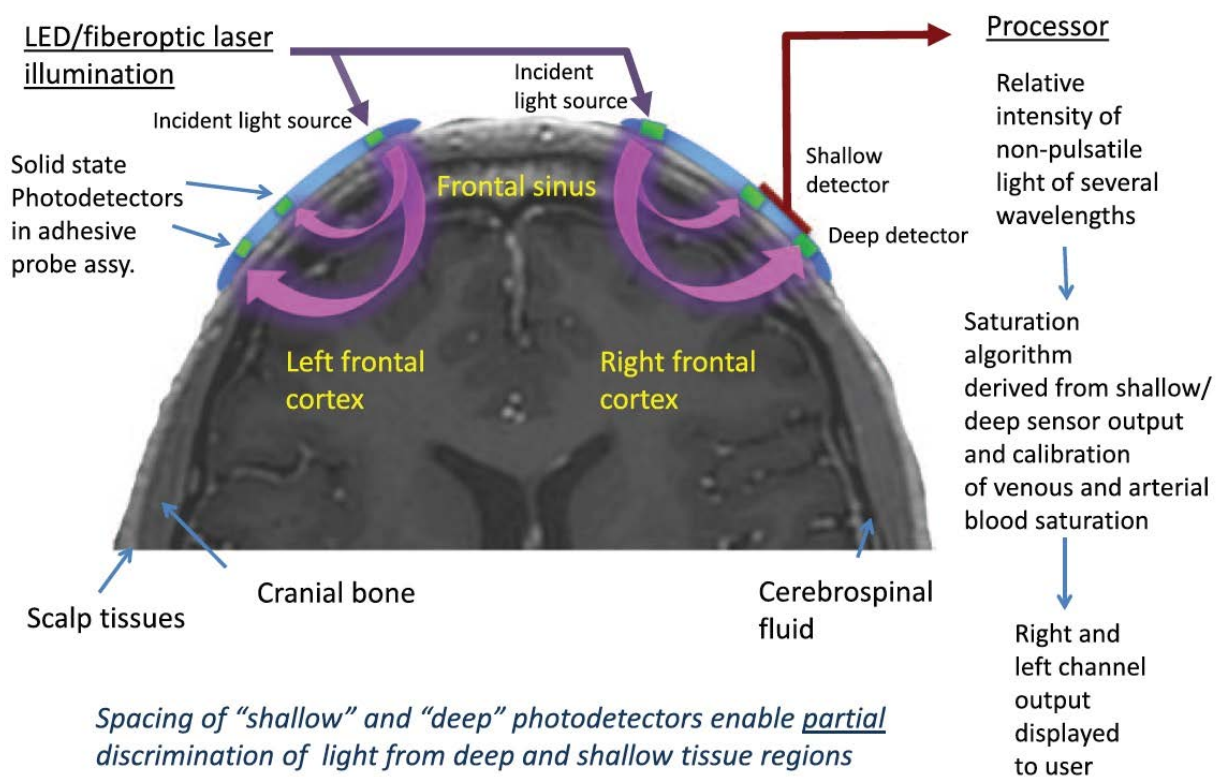
4) Concentrations Are Then Estimated Based On Absorbance / Optical Density At Various Wavelengths



$$[\text{Compound X}] = c_{11} \cdot \text{OD1} + c_{12} \cdot \text{OD2} + c_{13} \cdot \text{OD3} + c_{14} \cdot \text{OD4} + c_{15} \cdot \text{OD5} + c_{16} \cdot \text{OD6}$$

Appendix 3, Figure 3

Brain tissue hemoglobin oxygen saturation with near infrared spectroscopy



Appendix 3, Figure 1. Cerebral Blood Flow: an important feature of cerebral oximeters is their inability to differentiate between arterial, capillary, and venous blood. Red and infrared light are transmitted through, and absorbed by, arterial, capillary, and venous blood indiscriminately. Changes in the relative sizes of these compartments can therefore change the cerebral saturation calculation.

Appendix 3, Figure 2. How NIRS Works (Mathematics): cerebral oximeters use matrix algebra to estimate the relative concentration of distinct chromophores (e.g. oxy-hemoglobin, deoxy-hemoglobin). At least one wavelength of light is needed for each chromophore. Thus, at a minimum, a cerebral oximeter requires two wavelengths of light.

Appendix 3, Figure 3. How NIRS Works (Mechanics): in order to estimate the concentration of oxy-hemoglobin, deoxy-hemoglobin in the brain, cerebral oximeters utilize at least two sensors. Photons travel in a random path from their emitter, a light-emitting diode (LED), to each of the sensors. The “average” path of photons is affected by the distance between the LED and the sensors. Note that the path to the distal sensor passes through the brain, whereas the path to the proximal sensor does not. This difference allows these devices to mathematically remove the contribution of extracranial tissue to the calculation of ScO_2 , although because photons follow random paths and not perfect arcs (as depicted in Figure 2), this process is imperfect. Figure from Bickler P. et al., “Tissue Oximetry and Clinical Outcomes”, *Anesth Analg* 2017. Reproduced with permission.²³

References for Appendix 3: Detailed Description of Near-Infrared Spectroscopy (NIRS)

Devices

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Supplemental Tables

Supplemental Table 1: Pre-operative Baseline ScO₂ and Outcomes

| Author | Year | Population | n | Oximeter | Outcomes (in low ScO ₂ group) |
|-------------------------|------|--------------------------------|------|--------------------|---|
| Heringlake ¹ | 2011 | Cardiac surgery | 1178 | INVOS 4100 or 5100 | Increased 30-day mortality; composite [RRT, re-intubation, stroke, low CI, prolonged LOS] |
| Schoen ² | 2011 | Cardiopulmonary bypass | 231 | INVOS 5100 | Increased delirium |
| Sun ³ | 2014 | Cardiac surgery | 2097 | INVOS 5100c | Higher risk-adjusted mortality |
| Lei ⁴ | 2017 | Cardiopulmonary bypass | 249 | INVOS 5100c | Increased delirium (note, secondary analysis in negative RCT) |
| Ghosal ⁵ | 2018 | Left Ventricular Assist Device | 210 | INVOS 5100c | Increased 30-day mortality |

Supplemental Table 2: Case Reports of Intraoperative Use of Cerebral Oximetry

| Author | Year | Population | Oximeter | Findings |
|-------------------------|------|--|-----------------|--|
| Aono ^{*6} | 1998 | Aortic surgery | INVOS 3100 | ScO ₂ measurements were lower during circulatory arrest and increased to or above baseline during SCP (2 patients). |
| Blas ⁷ | 1999 | Aortic arch replacement | INVOS 3100 | Persistently reduced ScO ₂ prompted inspection of a malpositioned retrograde cerebral perfusion cannula. Following repositioning, ScO ₂ returned towards baseline. |
| Janelle ⁸ | 2002 | Repair of DeBakey type 1 aortic dissection | INVOS 5100 | Reduced ScO ₂ values during CPB led to surgical exploration identifying an extension of a false lumen into the carotid artery resulting in inadequate hemispheric cerebral blood flow. This was then surgically repaired. |
| Prabhune ⁹ | 2002 | Coronary artery bypass grafting | INVOS 4100 | Reduced ScO ₂ values during CPB led to identification of a gas leak from an anesthetic vaporizer manifold. |
| Sugawara ¹⁰ | 2002 | Ascending to infrarenal aortic bypass grafting | TOS-96 (TOSTEC) | ScO ₂ monitoring was utilized to guide rate of CPB flow to both reduce aortic pressure and prevent brain ischemia in complex surgery. |
| Han ¹¹ | 2005 | Total correction of tetralogy of Fallot | INVOS 5100 | ScO ₂ monitoring led to identification of a malpositioned superior vena cava cannula that was successfully repositioned. |
| Aron ¹² | 2007 | Coronary artery bypass grafting, mitral valve repair, modified MAZE procedure | INVOS 5100B | Reduced ScO ₂ measurements were attributed to Raynaud's disease episodes and managed with nitroglycerin administration. |
| Kasahara ¹³ | 2007 | Mitral valve repair | NIRO-200 | During CPB without aortic cross-clamping, aortic regurgitation during retraction of the atrial septum complicated surgical exposure. Hypothermic CPB with low flow was guided by monitoring of ScO ₂ values. |
| Cheng ¹⁴ | 2008 | Aortic arch replacement | INVOS 5100B | ScO ₂ trends were used to optimize cerebral perfusion and to confirm the patency of the surgical graft anastomosis. |
| Fujiwara ¹⁵ | 2008 | Mitral valve replacement (re-do) | Unknown | Reduced ScO ₂ was associated with anaphylactic shock caused by aprotinin. |
| Hassan ¹⁶ | 2010 | Mitral valve and aortic valve replacement | ForeSight® | A persistent left superior vena cava was incidentally found during surgery. ScO ₂ monitoring was used to indicate adequate cerebrovascular venous drainage following occlusion of the persistent left superior vena cava. |
| Paarmann ¹⁷ | 2010 | Transapical aortic valve replacement | INVOS 5100 | During cardiopulmonary resuscitation ScO ₂ trended in parallel with mixed venous oximetry. |
| Faulkner ¹⁸ | 2011 | Coronary artery bypass grafting, aortic valve replacement, mitral valve repair | ForeSight® | Reduced ScO ₂ led to identification of a malpositioned superior vena cava cannula. Upon correcting its position, ScO ₂ values returned to baseline. |
| Vernick ¹⁹ | 2011 | Coronary artery bypass grafting, aortic valve replacement, mitral valve repair | INVOS 5100 | Reduced ScO ₂ values following repair of the superior vena cava decannulation site after CPB led to diagnosis and subsequent repair of iatrogenic superior vena cava obstruction. |
| Chan ²⁰ | 2014 | Repair of type-A aortic dissection | INVOS | ScO ₂ monitoring identified a malpositioned catheter used for antegrade cerebral perfusion during deep hypothermic circulatory arrest. |
| Yamasaki ^{*21} | 2017 | Ross procedure | Unknown | Low ScO ₂ led to identification and repositioning of an aortic CPB cannula that had erroneously been placed in the left subclavian artery. |

DHCA=Deep Hypothermic Circulatory Arrest; SCP=Selective Cerebral Perfusion

*Article in Japanese – only the English-language abstract was reviewed. Table was adapted from Zheng 2013 (PMID 23267000) with additions.

Supplemental Table 3: Relationship Between Intraoperative Cerebral Desaturation and Outcomes

| Study | n | Oximeter | Outcome / test | Association between low (absolute) or decreased (trend) ScO ₂ and outcome | Comments |
|--------------------------------|-----|------------|--|--|--|
| Reents ²² | 47 | INVOS 4100 | cognitive decline (multiple tests) | No | ScO ₂ monitoring started after induction |
| Yao ²³ | 101 | INVOS 4100 | MMSE and ASEM 4-6 d post-OP | Yes | ScO ₂ cutoff 40% |
| Negargar ²⁴ | 72 | INVOS 4100 | MMSE 24h post-OP | No | Unplausible design |
| Hong ²⁵ | 100 | INVOS 5100 | Cognitive decline (various tests) / length of stay | No / Yes | LoS secondary outcome |
| Slater ²⁶ | 240 | INVOS 5100 | Cognitive decline (various tests) / length of stay | Yes | Change in study objectives from RCT to observational. Utilized a detaturation score indexing current ScO ₂ to average ScO ₂ throughout the procedure |
| de Tournay-Jetté ²⁷ | 61 | INVOS 5100 | Cognitive decline (various tests) | Yes | 1 month follow up |
| Schoen ²⁸ | 128 | INVOS 5100 | Cognitive decline (various tests)/complications | Yes /Yes | RCT – Sevoflurane vs. propofol - ScO ₂ effects detectable only in the TIVA group |
| Schoen ² | 231 | INVOS 5100 | Delirium / CAM/ICU | Yes | ScO ₂ effects detectable only in the pts. with ScO ₂ > 59.5% |
| Fischer ²⁹ | 30 | Foresight | Major complications | Yes | Dose dependent association between area under desaturation thresholds and complications |
| Kok ³⁰ | 60 | INVOS 5100 | Cognitive decline (multiple tests) | No | RCT of Off vs. On-pump CABG - only 3 patients with ScO ₂ < 40% for > 10 min. |
| Colak ³¹ | 190 | INVOS 5100 | Three cognitive function tests | Yes / Yes | Secondary analysis of RCT |
| Mukaida ³² | 573 | INVOS 5100 | Mortality | Yes / No | Baseline and lowest ScO ₂ were correlated with mortality, but not relative ScO ₂ |

Supplemental Table 4: Randomized Controlled Trials of Cerebral Oximetry in Cardiac Surgery

| Study | Year | n | Outcome / test | Positive effect of cerebral oximetry | Oximeter | Comments |
|-------------------------|------|-----|--|--------------------------------------|-----------------------------|--|
| Murkin ³³ | 2007 | 200 | MOMM | Yes | INVOS 5100 | Marginally significant combined endpoint |
| Mohandas ³⁴ | 2013 | 100 | MMSE / ASEM/ICU LOS | Yes | EQUANOX 7600 | 3 month follow up |
| Vretzakis ³⁵ | 2013 | 150 | No. of transfused PRC | Yes | INVOS 5100 | No oximetry in the control group |
| Colak ³¹ | 2014 | 190 | Cognitive decline (multiple tests) / LOS | Yes | INVOS 5100 | No oximetry in the control group |
| Harilal ³⁶ | 2014 | 40 | S100 beta | Yes | INVOS 5100 | No information on outcome |
| Kara ³⁷ | 2015 | 79 | Cognitive decline (multiple tests) / LOS | Yes | INVOS 5100 | No oximetry in the control group |
| Deschamps ³⁸ | 2016 | 201 | Reversibility of cerebral desaturation / morbidity and mortality | No | Multiple cerebral oximeters | Multicenter trial using different oximeters but a treatment algorithm developed for the INVOS oximeter (note: pilot study not powered for outcomes) |
| Lei ⁴ | 2017 | 249 | Delirium / CAM-ICU | No | INVOS 5100 | Baseline ScO ₂ predictive of delirium / 50% of patients premedicated with lorazepam / use of benzodiazepines intraoperative up to 0.05 mg/kg allowed but not reported |
| Rogers ³⁹ | 2017 | 208 | Cognitive decline (multiple tests) / morbidity and mortality | No | INVOS 5100 | Different minimal hematocrit goals in the control and intervention group / "generic- algorithm" in the control group not defined / intervention period limited to CPB period |

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